Altered Impulse Control in Alcohol Dependence: Neural Measures of Stop Signal Performance

Chiang-shan Ray Li, Xi Luo, Peisi Yan, Keri Bergquist, and Rajita Sinha

Background: Altered impulse control has been implicated in the shaping of habitual alcohol use and eventual alcohol dependence. We sought to identify the neural correlates of altered impulse control in 24 abstinent patients with alcohol dependence (PAD), as compared to 24 demographics matched healthy control subjects (HC). In particular, we examined the processes of risk taking and cognitive control as the neural endophenotypes of alcohol dependence.

Methods: To this end, functional magnetic resonance imaging (fMRI) was conducted during a stop signal task (SST), in which a procedure was used to elicit errors in the participants. The paradigm allowed trial-by-trial evaluation of response inhibition, error processing, and post-error behavioral adjustment. Furthermore, by imposing on the subjects to be both fast and accurate, the SST also introduced a distinct element of risk, which participants may or may not avert during the task. Brain imaging data were analyzed with Statistical Parametric Mapping in covariance analyses accounting for group disparity in general performance.

Results: The results showed that, compared to HC, PAD demonstrated longer go trial reaction time (RT) and higher stop success rate (SS%). HC and PAD were indistinguishable in stop signal reaction time (SSRT) and post-error slowing (PES). In a covariance analysis accounting for go trial RT and SS%, HC showed greater activity in the left dorsolateral prefrontal cortex than PAD, when subjects with short and long SSRT were contrasted. By comparing PAD and HC directly during stop errors (SE), as contrasted with SS, we observed greater activity in PAD in bilateral visual and frontal cortices. Compared to HC, PAD showed less activation of the right dorsolateral prefrontal cortex during PES, an index of post-error behavioral adjustment. Furthermore, PAD who showed higher alcohol urge at the time of the fMRI were particularly impaired in dorsolateral prefrontal activation, as compared to those with lower alcohol urge. Finally, compared to HC subjects, PAD showed less activity in cortical and subcortical structures including putamen, insula, and amygdala during risk-taking decisions in the SST.

Conclusion: These preliminary results provided evidence for altered neural processing during impulse control in PAD. These findings may provide a useful neural signature in the evaluation of treatment outcomes and development of novel pharmacotherapy for alcohol dependence.

Key Words: Alcohol Abuse, Impulsivity, Response Inhibition, Error Processing, go/nogo.

Alcohol dependence involves a wide range of serious medical and nonmedical conditions such as alcohol-related liver diseases, violence, and traffic accidents. Individuals as well as the society as a whole suffer a great deal from this serious mental illness. Understanding the psychological and neural processes leading to heavy, habitual, and eventually uncontrollable use of alcohol is thus an important public health issue and poses great challenges to addiction neuroscience.

A number of investigators have hypothesized a critical association between drug and alcohol addiction and deficits in impulse control (Ernst and Paulus, 2005; Everitt and Robbins, 2005; Goldstein and Volkow, 2002; Kalivas and Volkow, 2005; Moeller et al., 2001; Volkow and Li, 2005). Broadly defined in the literature, impulse control could comprise 2 distinguishable psychological dimensions. On one hand, impulse control implies ability to avoid risk and to curb excessive desire to seek sensation (Finn, 2002; Kelley et al., 2004; Kreek et al., 2005; Verdejo-Garcia et al., 2008). On the other hand, impulse control implies cognitive operations that allow individuals to change behaviors in a dynamic fashion on the basis of advance information or feedback derived from monitoring ongoing behavior (Botvinick et al., 2001; Carter et al., 1999; Kok et al., 2006; Ridderinkhof et al., 2004). This latter capability has specifically been referred to as cognitive control. By setting goals, inhibiting habitual acts, and monitoring performance, cognitive control allows behavioral flexibility for one to maneuver changing environment and optimize goal-directed actions (Dulley et al., 2004). Cognitive control thus serves to maintain homeostasis by a process that accommodates changing states of the decision maker (Paulus, 2007). It has been hypothesized that disrupted impulse control
along with heightened salience attributed to alcohol could lead to a vicious cycle of withdrawal, craving, bingeing, and intoxication (Goldstein and Volkow, 2002).

In this study, we employed the stop signal task (SST) as a behavioral proxy to explore whether neural process associated with impulsivity are altered in patients in alcohol dependence (PAD). The SST is widely used in the cognitive and imaging neuroscience literature (Logan, 1994; Logan and Cowan, 1984). In a “tracking” SST in which the difficulty of the stop trials were adjusted according to participants’ performance, we delineated the neural correlates of response inhibition, error processing, and post-error behavioral adjustment, which are key component processes of cognitive control (Li et al., 2006a, 2008a,b,c). Furthermore, by imposing on the participants to be both fast and accurate, the SST introduced a component of risk, which participants may avert by slowing down, or ignore by responding “as usual,” during go trials. We observed greater activity in a number of cortical and subcortical structures including the amygdala when participants take risk compared with when they avoid risk (Li et al., 2009). Thus, with the SST that allowed us to examine the neural processes of cognitive control and risk taking, we sought to establish a neural signature of impaired impulse control in PAD.

**MATERIALS AND METHODS**

**Subjects, Informed Consent, and Assessment of Alcohol Urge**

Twenty-four abstinent patients with alcohol dependence (PAD, 6 women) and 24 age- and education-matched HC subjects (6 women) participated in the study (Table 1). PAD met criteria for current alcohol dependence, as diagnosed by the Structured Clinical Interview for DSM-IV (First et al., 1995). PAD did not meet current DSM-IV criteria for dependence on other psychoactive substances, other than nicotine, and were also excluded if they met current criteria for any DSM IV Axis I psychiatric disorder. Recent use of other illicit substances was ruled out by urine toxicology screens upon admission. Women were excluded from the study if there were using any form of birth control or were either peri or postmenopausal. In addition, individuals with current depressive or anxiety symptoms requiring treatment or currently being treated for these symptoms were excluded as well. They were drug-free while staying in an inpatient treatment unit prior to the current fMRI study. All subjects were physically healthy with no major medical illnesses or current use of prescription medications. None of them reported having a history of impulsivity, head injury or neurological illness. The Human Investigation committee at Yale University School of Medicine approved all study procedures, and all subjects signed an informed consent prior to study participation.

Patients with alcohol dependence were assessed for their alcohol urge with the Alcohol Urge Questionnaire (AUQ; Bohn et al., 1995). AUQ was used to measure current alcohol urge on a Likert scale ranging from 1 (strongly disagree) to 7 (strongly agree), with a total of 8 items addressing desire for drink, expectation of positive affect from drinking, and inability to avoid drinking if alcohol was available. PAD were assessed with AUQ every 3 to 4 days during their inpatient stay. PAD participated in the fMRI study between 11 to 17 days (average = 2 weeks) after admission.

**Behavioral Task and Experimental Procedures**

We employed a simple reaction time (RT) task in this stop-signal paradigm (Fig. 1). There were 2 trial types: “go” and “stop,” randomly intermixed. A small dot appeared on the screen to engage attention and eye fixation at the beginning of a go trial. After a randomized time interval (fore-period) anywhere between 1 and 5 seconds, the dot turned into a circle, prompting the subjects to quickly press a button. The circle vanished at button press or after 1 second had elapsed, whichever came first, and the trial terminated. A premature button press prior to the appearance of the circle also terminated the trial. Three quarters of all trials were go trials. In a stop trial, an additional “X,” the “stop” signal, appeared after the go signal. The subjects were told to withhold button press upon seeing the stop signal. Likewise, a trial terminated at button press or when 1 second had elapsed since the appearance of the stop signal. The stop trials constituted the remaining ¼ quarter of the trials. There was an inter-trial interval of 2 seconds.

The time interval between the stop and the go signals (or the stop-signal delay; SSD) started at 200 milliseconds and varied from 1 stop trial to the next according to a staircase procedure: if the subject succeeded in withholding the response, the SSD increased by 64 milliseconds, making it more difficult for them to succeed again in the next stop trial; conversely, if they failed, SSD decreased by 64 milliseconds, making it easier for the next stop trial. With the staircase procedure, a “critical” SSD could be computed that represents the time delay required for the subject to succeed in withholding a response half of the time in the stop trials (Levitt, 1970). One-way to understand the SST is in terms of a horse race model with a go process and a stop process racing toward a finishing line (Logan, 1994). The go process prepares and generates the movement while the stop process inhibits movement initiation; whichever process finishes first determines whether a response will be initiated or not. Importantly, the go and stop processes race toward the activation threshold independently. Thus, the time required for the stop signal to be processed so a response is withheld (i.e., stop-signal

**Table 1. Demographics of the Subjects**

<table>
<thead>
<tr>
<th>Subject characteristic</th>
<th>PAD (n = 24)</th>
<th>HC (n = 24)</th>
<th>p value</th>
</tr>
</thead>
<tbody>
<tr>
<td>Men/women</td>
<td>18/6</td>
<td>18/6</td>
<td>0.13*</td>
</tr>
<tr>
<td>Age (years)</td>
<td>38.7 ± 8.3</td>
<td>35.5 ± 5.9</td>
<td></td>
</tr>
<tr>
<td>Ethnicity</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>African American</td>
<td>7 (29.2%)</td>
<td>5 (20.8%)</td>
<td>0.22a</td>
</tr>
<tr>
<td>Caucasian</td>
<td>17 (70.8%)</td>
<td>19 (79.2%)</td>
<td></td>
</tr>
<tr>
<td>Education (years)</td>
<td>12.5 ± 1.7</td>
<td>13.1 ± 1.6</td>
<td>0.23a</td>
</tr>
<tr>
<td>Average number of days of alcohol use/month prior to admission</td>
<td>24.2 ± 8.3</td>
<td>4.3 ± 3.1</td>
<td>&lt;0.0001b</td>
</tr>
<tr>
<td>Average number of years of alcohol use</td>
<td>10.2 ± 7.3</td>
<td>5.7 ± 4.5</td>
<td>&lt;0.0001a</td>
</tr>
</tbody>
</table>

*Notes: PAD, patients of alcohol dependence. Values are mean ± SD; *2-sample t-test; abinomial test; ddata not available in 2 healthy controls.*
reaction time or SSRT) can be computed on the basis of the go trial RT distribution and the odds of successful inhibits for different time delays between go and stop signals. This is performed by estimating the critical SSD at which a response can be correctly stopped in approximately 50% of the stop trials. With the assumptions of this “horse-race” model, the SSRT could then be computed for each individual subject by subtracting the critical SSD from the median RT distribution and the odds of successful inhibits for different times.

Subjects were instructed to respond to the go signal quickly while keeping in mind that a stop signal could come up in a small number of trials. Prior to the fMRI study each subject had a practice session outside the scanner. Each subject completed four 10-minute runs of the task with the SSD updated manually across runs. Depending on the actual stimulus timing (e.g., trials varied in fore-period duration) and speed of response, the total number of trials varied slightly across subjects in an experiment. With the staircase procedure we anticipated that the subjects would succeed in withholding their response in approximately 50% of the stop trials. This was thus an event-related fMRI study, with the go and stop trials randomly jittered to improve the efficiency of the study design.

We computed the fore-period effect as an index of motor preparedness during the SST (Li et al., 2005, 2006a; Tseng and Li, 2008). Briefly, longer fore-period is associated with faster response time (Bertelson and Tisseyre, 1968; Woodrow, 1914). Thus, RT of go trials with a fore-period between 3 and 5 seconds was compared with those with one between 1 and 3 seconds, and the effect size of RT difference was defined as fore-period effect. It is also known that in a RT task the RT of a correct response is prolonged following an error, compared with other correct responses, and this prolonged RT is thought to reflect cognitive processes involved in error monitoring (Rabbit, 1966). We thus computed the RT difference between the go trials that followed a stop error (SE) and those that followed another go trial, and termed this RT difference “post-error slowing” (PES) (Hajcak et al., 2003; Li et al., 2008a).

**Imaging Protocol**

Conventional T1-weighted spin echo sagittal anatomical images were acquired for slice localization using a 3T scanner (Siemens Trio, Erlangen, Germany). Anatomical images of the functional slice locations were next obtained with spin echo imaging in the axial plane parallel to the AC–PC line with repetition time (TR) = 300 milliseconds, echo time (TE) = 2.5 milliseconds, bandwidth = 300 Hz/pixel, flip angle = 60°, field of view = 220 × 220 mm, matrix = 256 × 256, 32 slices with slice thickness = 4 mm and no gap. Functional, blood oxygenation level dependent (BOLD) signals were then acquired with a single-shot gradient echo-echo-planar imaging (EPI) sequence. Thirty-two axial slices parallel to the AC–PC line covering the whole brain were acquired with TR = 2,000 milliseconds, TE = 25 milliseconds, bandwidth = 2,004 Hz/pixel, flip angle = 85°, field of view = 220 × 220 mm, matrix = 64 × 64, 32 slices with slice thickness = 4 mm and no gap. Three hundred images were acquired in each run for a total of 4 runs.

**Data Analysis and Statistics**

Data were analyzed with Statistical Parametric Mapping version 2 (Wellcome Department of Imaging Neuroscience, University College London, UK). Images from the first 5 TRs at the beginning of each trial were discarded to enable the signal to achieve steady state equilibrium between radiofrequency (RF) pulsing and relaxation. Images of each individual subject were first corrected for slice timing and realigned (motion corrected). A mean functional image volume was constructed for each subject for each run from the realigned image volumes. These mean images were normalized to a Montreal Neurological Institute EPI template with affine registration followed by nonlinear transformation (Ashburner and Friston, 1999; Friston et al., 1995a). The normalization parameters determined for the mean functional volume were then applied to the corresponding functional image volumes for each subject. Finally, images were smoothed with a Gaussian kernel of 10 mm at full width at half maximum. The data were high-pass filtered (1/128 Hz cutoff) to remove low-frequency signal drifts.

Four main types of trial outcome were distinguished: go success (G), go error (F), stop success (SS), and SE trial (Fig. 1). A statistical analytical design was constructed for each individual subject, using the general linear model (GLM) with the onsets of go signal in each of these trial types convolved with a canonical hemodynamic response function (HRF) and with the temporal derivative of the canonical HRF and entered as regressors in the model (Friston et al.,

![Fig. 1. (A) Stop signal paradigm. In “go” trials (75%) observers responded to the go signal (a circle) and in “stop” trials (25%) they had to withhold the response when they saw the stop signal (an X). In both trials the go signal appeared after a randomized time interval between 1 and 5 seconds (the fore-period or FP) following the appearance of the fixation point. The stop signal followed the go signal by a time delay—the stop-signal delay (SSD). The SSD was updated according to a staircase procedure, whereby it increased and decreased by 64 milliseconds following a stop success (SS) and stop error (SE) trial, respectively. (B) An example sequence of trials to illustrate the definition of post-go slowing versus post-go speeding in go trial reaction time; and post-error slowing versus post-error speeding in go trial reaction time.](image-url)
1995b). Realignment parameters in all 6 dimensions were also entered in the model. Serial autocorrelation was corrected by a first-degree autoregressive 1 model. The GLM estimated the component of variance that could be explained by each of the regressors. We constructed for each individual subject statistical contrasts: SS > SE and SE > SS.

In a second GLM, G, F, SS, and SE trials were first distinguished. G trials were divided into those that followed a G (pG), SS (pSS), and SE (pSE) trial. Furthermore, pSE trials were divided into those that increased in RT (pSEi) and those that did not increase in RT (pSEni), to allow the isolation of neural processes involved in post-error behavioral adjustment (Li et al., 2008a). To determine whether a pSE trial increased or did not increase in RT, it was compared with the pG trials that preceded it in time during each session. The pG trials that followed the pSE trial were not included for comparison because the neural/cognitive processes associated with these pG trials occurred subsequent to and thus could not have a causal effect on the pSE trial (Li et al., 2008a). We constructed for each individual subject 2 contrasts: SS > SE to compare, with the first GLM and verify the model; and pSEi versus pSEni, to identify activations associated with PES.

In this second GLM, pG trials were also divided into those that increased in RT (pGi) and those that did not increase in RT (pGni; Li et al., 2009). Similarly, to determine whether a pG trial increased or did not increase in RT, it was compared with the pG trials that preceded it in time during each session. We contrasted pGni > pGi (i.e., post-go speeding > post-go slowing) for each individual subject to identify activations associated with risk-taking decisions in the SST.

Random Effect Analyses of Brain Imaging Data

Response Inhibition. The SS and SE trials were identical in stimulus condition, with SS trials involving inhibition success and SE trials involving inhibition failure. The contrast SS > SE thus engaged processes related to response inhibition and was used in the random effect analysis (Li et al., 2006a). With the SSRT to index response inhibition, PAD and HC were each grouped into those with short (n = 12) and long (n = 12) SSRT on the basis of a median split, following the rationale of the race model (Li et al., 2006a; Logan, 1994). In a 2 x 2 ANOVA, the contrasts HC > PAD (short > long SSRT) allowed us to identify structures showing greater activation in HC when compared with PAD during response inhibition and vice versa.

Error Processing. We compared PAD and HC using the contrast SE > SS in a covariance analysis accounting for go trial RT and SS%.

Post-Error Slowing. We compared PAD and HC using the contrast pSEi > pSEni in a covariance analysis accounting for go trial RT and SS%.

Risk Taking. We compared PAD and HC using the contrast pGni > pGi in a covariance analysis accounting for go trial RT and SS%.

In addition to voxelwise whole brain exploration, we also performed region of interest (ROI) analysis based on our previous findings (Li et al., 2006a, 2008a,b, 2009). We used MarsBaR (Brett et al., 2002; http://www.marsbar.sourceforge.net/) to compute for each individual subject the effect size (t statistic) of activity change for functional ROIs derived from our published studies. The effect size rather than mean difference in brain activity was derived in order to account for individual differences in the variance of the mean. These ROIs included 2 cortical regions related to response inhibition (Li et al., 2006a): the dorsal medial frontal cortex (dmFC; x = -4, y = 32, z = 51) and the other focused on the rostral anterior cingulate cortex (rACC; x = -8, y = 35, z = 19); and the left caudate head (Li et al., 2008c). Seven regions related to error processing were also designated as ROIs (Li et al., 2008b): dorsal anterior cingulate cortex (ACC; x = -4, y = 16, z = 44) extending to supplemento motor area; cuneus including retrosplenial cortex (x = 16, y = -64, z = 8); thalamus (x = -12, y = -16, z = 8); left insula probably including inferior frontal cortex (x = -48, y = 8, z = -8); superior frontal and precentral gyrus (x = -36, y = -8, z = 52); superior temporal gyrus (x = -48, y = -28, z = 24); and right insula (x = 44, y = 16, z = 0). One region related to PES was identified as an ROI (Li et al., 2008a): ventrolateral prefrontal cortex (VLPFC, x = 44, y = 24, z = -4; BA 47). Finally, 2 regions related to risk taking were identified as ROIs (Li et al., 2009): amygdala (x = -16, y = -4, z = -16) and the posterior cingulate cortex (PCC; x = -4, y = -40, z = 44).

**RESULTS**

Behavioral Performance

Table 2 summarizes the stop signal performance for PAD and HC. Compared with HC, PAD were significantly slower in median go trial RT, suggesting that they adopted a more conservative response strategy. PAD also showed a higher SS rate, compared with HC. The results suggested that, compared with HC, PAD exercised greater attention in monitoring for the stop signal. This discrepancy in attentional monitoring thus needed to be accounted for when regional brain activities were compared for response inhibition and PES. The 2 groups otherwise did not differ in stop signal performance. Furthermore, PAD demonstrated an average of 78 ± 20 milliseconds in post-go speeding in RT and 93 ± 18 milliseconds in post-go slowing in RT, not differently from HC, who demonstrated an average of 85 ± 15 milliseconds in post-go speeding in RT and 92 ± 18 milliseconds in post-go slowing in RT.

**Table 2.** General Performance in the Stop Signal Task

<table>
<thead>
<tr>
<th>Group</th>
<th>Median go RT (milliseconds)</th>
<th>%go</th>
<th>%stop</th>
<th>SSRT (milliseconds)</th>
<th>FP effect(^a) (effect size)</th>
<th>PES (effect size)</th>
<th>RT difference between pG speeding and slowing (milliseconds)(^a)</th>
</tr>
</thead>
<tbody>
<tr>
<td>PAD</td>
<td>687 ± 114</td>
<td>96.2 ± 1.63</td>
<td>53.3 ± 3.6</td>
<td>190 ± 30</td>
<td>1.78 ± 1.68</td>
<td>1.56 ± 2.06</td>
<td>-171 ± 33</td>
</tr>
<tr>
<td>HC</td>
<td>595 ± 150</td>
<td>96.5 ± 1.81</td>
<td>50.9 ± 2.6</td>
<td>195 ± 36</td>
<td>2.27 ± 1.65</td>
<td>1.42 ± 1.52</td>
<td>-181 ± 49</td>
</tr>
<tr>
<td>p value</td>
<td>0.020*</td>
<td>0.850</td>
<td>0.010*</td>
<td>0.645</td>
<td>0.310</td>
<td>0.791</td>
<td>0.386</td>
</tr>
</tbody>
</table>

Notes: PAD, patients with alcohol dependence; HC, healthy controls; %go and %stop, percentage of successful go and stop trials; SSRT, stop-signal reaction time; FP, fore-period effect: 42 ± 42 milliseconds (AD) versus 54 ± 34 milliseconds (HC); PES, post-error slowing: 38 ± 51 milliseconds (AD) versus 36 ± 37 milliseconds (HC). All numbers are mean ± SD; p value based on 2-tailed 2 sample t-test, *<0.05; \(^a\)pG: post-go = extent of post-go speeding – extent of post-go slowing. See text for further explanation.
-82 ± 26 milliseconds in post-go speeding in RT and 99 ± 25 milliseconds in post-go slowing in RT.

Table 3 summarizes the stop signal performance separately for short and long SSRT group each for PAD and HC. PAD and HC showed near-trend and trend difference in median go trial RT and SS rate.

Other analyses indicated that performance of both PAD and HC was well tracked by the staircase procedure. These findings included that both PAD and HC subjects succeeded in approximately half of the stop trials; and both showed a significant linear correlation between the RT of SE trials and the SSD ($p < 0.005, 0.446 < R < 0.941$, Pearson regression; Logan and Cowan, 1984).

Table 3. General Performance of PAD and HC in the Stop Signal Task, Grouped by SSRT

<table>
<thead>
<tr>
<th>Group</th>
<th>SSRT (milliseconds)</th>
<th>Median go RT (milliseconds)</th>
<th>%go</th>
<th>%stop</th>
<th>FP effect (effect size)</th>
<th>PES (effect size)</th>
</tr>
</thead>
<tbody>
<tr>
<td>PAD, short</td>
<td>170 ± 18</td>
<td>743 ± 77</td>
<td>95.5 ± 1.1</td>
<td>54.6 ± 4.1</td>
<td>1.77 ± 1.63</td>
<td>0.89 ± 2.11</td>
</tr>
<tr>
<td>PAD, long</td>
<td>211 ± 25</td>
<td>632 ± 120</td>
<td>96.8 ± 1.8</td>
<td>51.9 ± 2.4</td>
<td>1.78 ± 1.81</td>
<td>2.23 ± 1.85</td>
</tr>
<tr>
<td>HC, short</td>
<td>168 ± 25</td>
<td>593 ± 166</td>
<td>96.1 ± 1.7</td>
<td>50.7 ± 3.2</td>
<td>2.08 ± 1.11</td>
<td>1.26 ± 1.85</td>
</tr>
<tr>
<td>HC, long</td>
<td>222 ± 22</td>
<td>597 ± 138</td>
<td>96.9 ± 1.9</td>
<td>51.1 ± 1.8</td>
<td>2.46 ± 2.09</td>
<td>1.58 ± 1.17</td>
</tr>
<tr>
<td>p value, interaction effect</td>
<td>0.327</td>
<td>0.131</td>
<td>0.623</td>
<td>0.076</td>
<td>0.703</td>
<td>0.322</td>
</tr>
</tbody>
</table>

**Notes:** PAD, patients with alcohol dependence; HC, healthy controls; %go and %stop, percentage of successful go and stop trials; SSRT, stop-signal reaction time; PES, post-error slowing; all numbers are mean ± SD; $p$ values of the interaction effect are all based on 2-way ANOVA: subject by SSRT group.

Whole Brain and Region of Interest Analyses

We applied the same threshold of $p < 0.001$, uncorrected and 5 voxels in the extent of activation to all second-level whole brain analyses of imaging data. In ROI analyses, a threshold of $p < 0.05$, uncorrected was first set up for the whole brain exploration, and the results were reported with small volume correction using $p < 0.001$, uncorrected.

**Response Inhibition.** PAD and HC were compared for the contrast SS > SE, in a group (PAD vs. HC) by SSRT (short vs. long) ANOVA. The results showed greater activation in the short as contrasted to long SSRT group in HC compared with PAD in the left dorsolateral prefrontal cortex (DLPFC, $x = -48, y = 24, z = 36, Z = 3.70$, 8 voxels, Fig. 2). Since the 2 SSRT groups showed near-trend or trend differences in go trial RT and SS%, we performed another ANOVA co-varied for these 2 variables. The results were essentially identical: HC showed greater left DLPFC activity ($x = -48, y = 24, z = 36, Z = 3.57$, 5 voxels). PAD did not show greater regional brain activity than HC for the same contrast. In ROI analyses, PAD and HC did not differ in the dmFC, rACC, left caudate head masks in the same ANOVA.

**Error Processing.** Contrasting SE with SS trials, PAD showed increased activity compared with HC in a number of brain regions including bilateral visual and frontal cortices in a 2-sample $t$-test (Fig. 3; Table 4). Conversely, no brain regions showed greater activity in the same covariance analysis in HC, when compared with PAD. In ROI analysis for error processing, PAD and HC did not show differential activity in any of the 7 masks identified from our earlier studies.

**Post-Error Slowing.** Compared with HC, PAD showed less activation of the right DLPFC ($x = 44, y = 32, z = 40$, $Z = 3.62$, 14 voxels; Fig. 4) during post-SE go trials with RT increase (pSEi) contrasted with post-SE go trials without RT increase (pSEni); i.e., PES. No brain regions showed greater activity during PES in PAD when compared with HC. In ROI analysis, we compared PAD and HC for pSEi > pSEni on the basis of small volume correction for the right VLPFC mask. The results showed that PAD and HC did not differ in activation for this contrast in right VLPFC.

**Risk Taking.** PAD and HC were compared for the contrast: post-go go trials without RT increase (pGni) > post-go go trials with RT increase (pGi). The results showed decreased activation in a number of cortical and subcortical...
structures including the putamen and insula in PAD, compared with HC (Fig. 5; Table 5). In ROI analyses, we compared PAD and HC for pGni > pGi for a mask of the amygdala and the PCC. The results showed that, compared with HC, PAD demonstrated decreased activation in the amygdala \( p < 0.025 \), corrected for family-wise error (FWE), \( Z = 2.64, x = -20, y = -4, z = -16 \) and in the PCC \( p < 0.030 \), corrected for FWE, \( Z = 2.62, x = -8, y = -36, z = 44 \).

**Correlation of Neural Measures With Alcohol Use in PAD**

Linear regression analyses indicated that left DLPFC activity during response inhibition, right DLPFC activity during PES, amygdala or PCC/precuneus activity during risk taking, or any of the regional activities during error processing did not correlate with years of alcohol use or the total amount of alcohol use in the 90 days prior to admission in the PAD \( -0.122 < r < 0.025; 0.122 < p < 0.571 \).

**Comparing PAD With High and Low Alcohol Urge Rating**

Patients of alcohol dependence showed a rating of 20.3 ± 15.0 (mean ± SD; range: 8 to 50) on alcohol use urge based on the AUQ on the first day of admission. Alcohol urge decreased over a course of 4 to 5 weeks of inpatient stay. Because of varying alcohol urge rating across individuals, we normalized the ratings to individual means to obtain a relative measure of alcohol urge. Functional MR scans were performed between days 11 and 17 after admission, a period when the average relative urge was under 1.0. However, individual PAD varied in alcohol urge, with 5 PAD showing a relative urge greater than 1.0 (high urge group) and 19 PAD showing a relative urge less than 1.0 (low urge group) at the time when fMRI was conducted (1.18 ± 0.16 vs. 0.86 ± 0.14, \( p < 0.001 \), 2-sample t-test).

We compared these 2 groups of PAD for the effect size of activity changes for the left DLPFC (response inhibition), right DLPFC (PES), amygdala, and PCC (risk taking) that showed differential activity between PAD and HC. Because of multiple comparisons, we guarded against false positive

### Table 4. Brain Regions Showing Greater Activity in PAD, Compared With HC, During Stop Error > Stop Success

<table>
<thead>
<tr>
<th>Cluster size (voxels)</th>
<th>Voxel Z value</th>
<th>x</th>
<th>y</th>
<th>z</th>
<th>Identified brain region</th>
</tr>
</thead>
<tbody>
<tr>
<td>49</td>
<td>4.39</td>
<td>-56</td>
<td>-72</td>
<td>12</td>
<td>Middle temporal G</td>
</tr>
<tr>
<td>24</td>
<td>4.30</td>
<td>20</td>
<td>-64</td>
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<tr>
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<td>56</td>
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<tr>
<td>115</td>
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<td>36</td>
<td>-84</td>
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<td>Intraoccipital sulcus/superior occipital G</td>
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<td>Inferior precentral S/middle frontal G</td>
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<td>-12</td>
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<td>Cingulate G</td>
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<td>7</td>
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<td>12</td>
<td>-40</td>
<td>72</td>
<td>Paracentral lobule</td>
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</tbody>
</table>

Notes: PAD, patients of alcohol dependence; HC, healthy controls; G, gyrus; S, sulcus; MNI, Montreal Neurological Institute.
results at an \( z \) of 0.012. The results showed that, compared with the low urge group, the high urge group showed significantly less activity in the right DLPFC during PES (effect size: \(-1.54 \pm 0.91 \) vs. \( 0.45 \pm 1.37, p < 0.006; 2\text{-sample} t\text{-test})

**DISCUSSION**

Prefrontal Functions, Cognitive Control, and Alcohol Dependence

Chronic and heavy alcohol use is known to be associated with a wide range of altered cognitive and affective states (Sullivan and Pfefferbaum, 2005; Sher, 2006). A number of functional imaging studies have examined the neural processes underlying motor dysfunction (Parks et al., 2003), working memory dysfunction (Akine et al., 2007; Caldwell et al., 2005; Schweinsburg et al., 2005; Tapert et al., 2004a), cue-elicited craving (Filbey et al., 2008; Grüsser et al., 2004; Heinz et al., 2004; Myrick et al., 2004; Park et al., 2007; Tapert et al., 2004a, 2003, 2004b; Wrase et al., 2002, 2007), altered perceptual detection (Hermann et al., 2007), and affective processing (Heinz et al., 2007; Salloum et al., 2007) in alcohol-dependent patients. Some have specifically addressed altered inhibitory control in these patients (Anderson et al., 2005; Karch et al., 2008; Schweinsburg et al., 2004). For instance, Anderson and colleagues (2005) showed that greater BOLD response to inhibition during a go/nogo task predicted more expectancies of cognitive and motor impairment from alcohol in adolescents who were assessed with alcohol expectancies. These results suggested that decreased inhibitory control may contribute to more positive and less negative expectancies, which could eventually lead to problem drinking (Anderson et al., 2005).

The current study assessed impulse control in PAD using the SST. In particular, we attempted to examine cognitive control independent of general task performance. On the basis of our previous findings from the same behavioral paradigm in healthy individuals, we sought to identify altered cerebral processes in PAD during component processes of cognitive control (Li and Sinha, 2008). Overall, our results suggested that PAD showed altered activity in a number of cortical structures during response inhibition, error processing, and post-error behavioral adjustment. In particular, the findings of decreased dorsolateral prefrontal cortical activation during response inhibition and PES are broadly in accord with previous studies demonstrating altered prefrontal cortical activity in patients with alcohol misuse (Akine et al., 2007; Bowden-Jones et al., 2005; Chanraud et al., 2007; Clark et al., 2007; Dao-Castellana et al., 1998; De Bellis et al., 2005; de Greck et al., 2009; Fein et al., 2006; Goldstein et al., 2004; Heinz et al., 2007; Pfefferbaum et al., 2001; Rupp et al., 2006; Scheックmann et al., 2007; Verdejo-García et al., 2006; see also Kopelman, 2008; Scheurich, 2005; Sinha and Li, 2007; Uekermann and Daum, 2008, for a review). For instance, the finding of decreased left DLPFC activation during response inhibition in PAD when compared with HC is consistent with an earlier report showing diminished activity in the same brain region in chronic alcoholics during performance of the Stroop test (Dao-Castellana et al., 1998). Our finding of decreased right DLPFC activity during PES is also consistent with an earlier study of alcoholic patients showing decreased bilateral
DLPFC activation during a working memory task (Pfefferbaum et al., 2001).

Altered prefrontal activity has been reported in alcoholic patients in response to alcohol cues and craving (George et al., 2001; Olbrich et al., 2006; Wilson et al., 2004). For instance, PAD showed increased activity in the DLPFC and anterior thalamus in response to alcohol cues when compared with control visual cues (George et al., 2001). Furthermore, transcranial electrical stimulation of the prefrontal cortices appeared to ameliorate alcohol craving in these patients (Boggio et al., 2008). Thus, the current findings of greater changes in prefrontal cortical activity in PAD with higher alcohol urge are broadly consistent with the idea of prefrontal regulation of alcohol craving (Sinha and Li, 2007). On the other hand, craving and cognitive control represent opposing constructs in theorizing the regulation of alcohol use behavior. One possibility is that cue induced prefrontal activation represents an inflow of subcortical activity form the reward and emotion circuits rather than a signal of top-down executive control during the cue induction paradigms (Boggio et al., 2008). Thus, although the current finding of prefrontal functional changes associated with alcohol urge highlighted a crucial aspect of prefrontal functions, further studies are required to clarify the specific roles of prefrontal cortices in the regulation of alcohol craving.

Previous evoked potential and fMRI studies have reported disrupted error-related brain activity and connectivity associated with alcohol consumption (Holroyd and Yeung, 2003; Meda et al., 2009; Ridderinkhof et al., 2002). For instance, moderate alcohol intake is associated with diminished error-related anterior cingulate activity and failure to initiate post-error behavioral adjustment in young adult social drinkers (Ridderinkhof et al., 2002). The present findings of greater error-related activity thus appeared to characterize a complementary profile of cerebral responses in PAD during a stage of early abstinence. Taken together, a contrasting pattern of decreased prefrontal activity during response inhibition and post-error behavioral adjustment and increased frontal including anterior cingulate activity during errors described our cohort of PAD during the SST. These results add to the evidence that prefrontal cortical functions may play a critical role in the shaping of alcohol dependence.

**Neural Processes of Risk Taking and Alcohol Dependence**

Compared with HC subjects, PAD showed less activation during risk-taking decisions in a number of cortical and subcortical structures. For instance, PAD showed less activation of the medial orbitofrontal cortex (mOFC), an area implicated in prediction error signaling and the detection of contingency change (Blair, 2007). Interestingly, the mOFC (in contrast to the lateral OFC) has also been shown to play a role in processing positive and rewarding information (Liu et al., 2007; Nieuwenhuis et al., 2005; O’Doherty et al., 2001). Thus, compared with HC subjects, PAD might experience post-go speeding, in contrast to post-go slowing, as a less rewarding event. Alcohol dependence is associated with a down regulation of circuit activity that is “normally” engaged when individuals partake in a risk-taking decision.

Risk taking also activates parietal cortex and the rACC, according to a meta-analysis of imaging studies involving decision making (Krain et al., 2006). Compared with HC subjects, PAD showed less activation of the bilateral parietal cortices and the rACC, suggesting that risk taking is a less salient event for the patients. Furthermore, our finding of decreased amygdala activity during risk-taking decisions in the SST is also consistent with the literature implicating this subcortical structure in alcohol misuse. For instance, alcohol abuse has also been associated with impaired amygdala processes during aversive learning (Stephens and Duka, 2008). Postmortem studies showed altered serotonergic neurotransmission in the amygdala, suggesting dysfunctional affect regulation in chronic alcoholics (Stovvik et al., 2007). Taken overall, these findings suggest that risk taking as a distinct dimension of

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**Table 5. Brain Regions Showing Greater Activity in HC, Compared With PAD, During Risk-Taking Decisions**

<table>
<thead>
<tr>
<th>Cluster size (voxels)</th>
<th>Voxel Z value</th>
<th>MNI coordinate (mm)</th>
<th>Identified brain region</th>
</tr>
</thead>
<tbody>
<tr>
<td>43</td>
<td>40.01</td>
<td>x = 40, y = -60, z = 0</td>
<td>Middle occipital/temporal G</td>
</tr>
<tr>
<td>23</td>
<td>3.84</td>
<td>x = 32, y = 40, z = 24</td>
<td>Middle frontal G</td>
</tr>
<tr>
<td>53</td>
<td>3.81</td>
<td>x = 24, y = 12, z = -12</td>
<td>Putamen</td>
</tr>
<tr>
<td>9</td>
<td>3.42</td>
<td>x = 40, y = -8, z = -16</td>
<td>Insula</td>
</tr>
<tr>
<td>23</td>
<td>3.68</td>
<td>x = 28, y = 36, z = -12</td>
<td>Medial orbital G</td>
</tr>
<tr>
<td>19</td>
<td>3.62</td>
<td>x = 44, y = -12, z = 64</td>
<td>Superior precentral sulcus/precentral G</td>
</tr>
<tr>
<td>27</td>
<td>3.55</td>
<td>x = 4, y = -88, z = -40</td>
<td>Cuneus/superior occipital G</td>
</tr>
<tr>
<td>9</td>
<td>3.51</td>
<td>x = -52, y = -52, z = -20</td>
<td>Middle temporal G</td>
</tr>
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<td>3.49</td>
<td>x = -52, y = -24, z = 44</td>
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<td>Lateral fissure/postcentral G</td>
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<td>3.34</td>
<td>x = 32, y = -68, z = 36</td>
<td>Intraparietal sulcus</td>
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<td>10</td>
<td>3.33</td>
<td>x = -4, y = 16, z = 40</td>
<td>Cingulate G/sulcus</td>
</tr>
</tbody>
</table>

*Notes: PAD, patients of alcohol dependence; HC, healthy controls; G, gyrus; MNI, Montreal Neurological Institute.*
impulse control does not evoke in PAD cerebral activity documented for healthy individuals. The SST appears to be a useful proxy to examine risk-related behavior as well as cognitive control.

Limitations of the Study and Conclusions

It is important to note a few limitations of the current study. First, although they do not meet criteria of another substance use disorder, many of our PAD used cocaine or other illicit substances. Because of the moderate sample size of the current study, we did not attempt to accommodate this and other clinical factors such as history of trauma and/or mood disorders, which may impact the neural measure of impulse control. Secondly, impulse control can be addressed in a number of behavioral tasks other than the stop signal paradigm. In particular, behavioral tasks incorporating an explicit component of reward, such as the delayed discounting task, would be of tremendous value in elucidating other aspects of impulse control impairment in alcohol dependence (Bjork et al., 2004; Field et al., 2007; Mitchell et al., 2005; Petry, 2001; Petry et al., 2002; Richards et al., 1999; Takahashi et al., 2007; Vuchinich and Simpson, 1998; see also Bickel et al., 2007, for a review). Thirdly, we conducted the fMRI study during a relatively early stage of abstinence in the PAD. Although the patients were free of symptoms and signs of acute alcohol withdrawal, they might continue to experience evolution of other alcohol-related mood states such as anxiety. Thus, studies would be warranted at a later stage of abstinence to confirm the present findings. Fourthly, because of the small number of women recruited for the study, we did not compare women and men subjects in the current study. However, we have previously noted gender differences in cognitive control during the SST (Li et al., 2006b). It would be important to further explore whether the gender differences in brain activation during the SST manifest in relation to alcohol dependence. Finally, PAD overall did not differ from HC in behavioral measures of impulse control. Therefore, the current results did not ascertain behavioral deficits in impulse control in PAD. Studies of a greater sample size are required in the future to further pursue this issue.

Despite these limitations, the current findings are to our knowledge the first to dissect the component processes of impulse control altered in alcohol dependence within a single behavioral paradigm. We confirmed prefrontal cortical deficits during cognitive control, highlighted a contrasting pattern of error-related activations, and elucidated a distinct dimension of risk taking, which may serve as useful neural markers of alcohol dependence.

ACKNOWLEDGMENTS

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